

# *The hypoglycaemia free artificial pancreas project*

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# Joint work with

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- Eric Le Carpentier
- ...

# content

- Some history/state of the art
- Mathematical model
- Identification
- Control
  
- The perspectives (hospital & industry...)

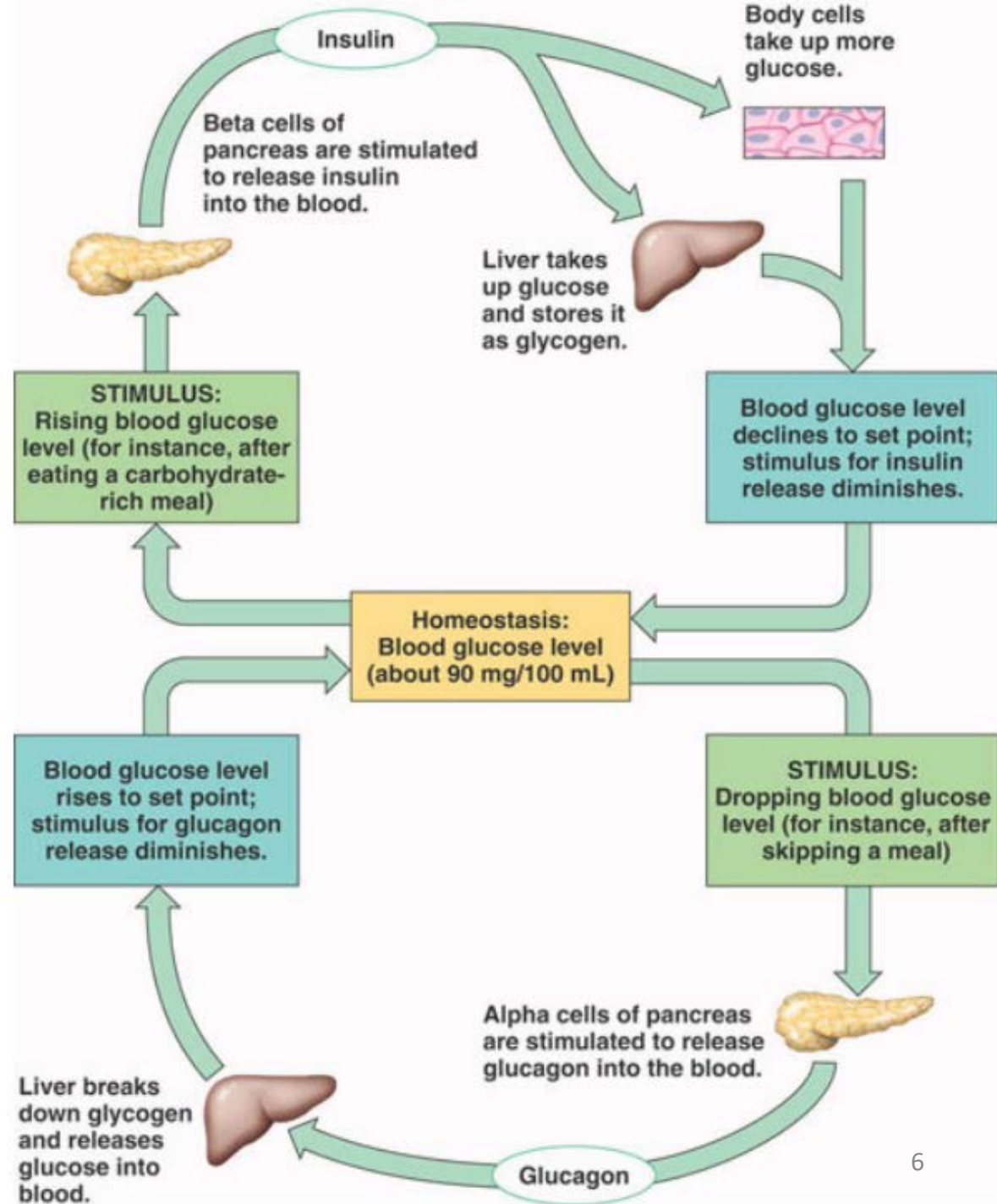
# Main message

- Stick to medical practice: FIT, Flexible Insulin Therapy  
→ Constraints on the model
  
- Avoid hypoglycemia  
→ Existing (Medtronic, Diabeloop) solutions may be open loop for up to 30% of the time

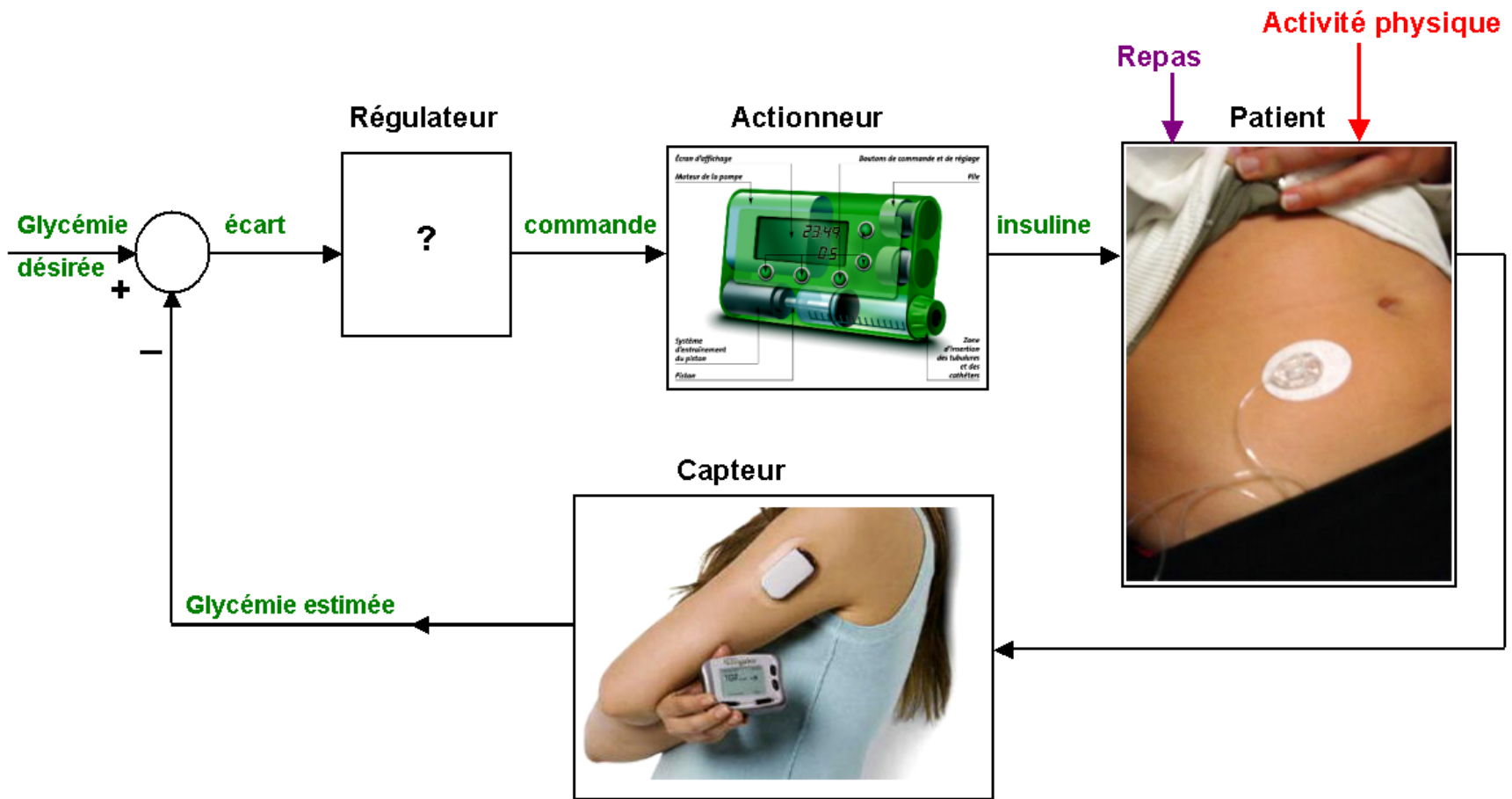
# The general population vs Diabetes

- No diabetes
- Type 1 → no insulin production by the pancreas
- Type 2 → aging patients, lack of insulin production, decrease of sensitivity
- diabetes related to pregnancy

Biology –  
the natural  
mechanism  
which  
regulates  
glycemia



# A challenging control problem



# Long standing contributions !

- PADOVA : C. Cobelli et al.
- Montpellier hospital : E. Renard
- ...
- > 1960's



# Our choices/constraints

- **Stick to medical practice:** FIT, Flexible Insulin Therapy
  - Recover the basal rate from the mathematical model
  - Definition - the basal insulin rate stabilizes any glucose concentration.*
- Avoid hypoglycemia
  - *Positivity of the system*

# Mathematical model

- Stick to medical practice: FIT, Flexible Insulin Therapy

If no meal & stable glycemia:

$$\dot{G} = 0$$

Or

$$\dot{G} = \theta(I_{basal} - I)$$

$$\dot{G} = \theta_1 - \theta_2 I$$

If a meal is ingested:

$$\dot{G} = \theta_1 - \theta_2 I + \theta_3 D$$

# Mathematical model

$$\dot{G} = \theta_1 - \theta_2 I + \theta_3 D$$

$\theta_1$  : glucose delivery from the liver – consumption by the brain...

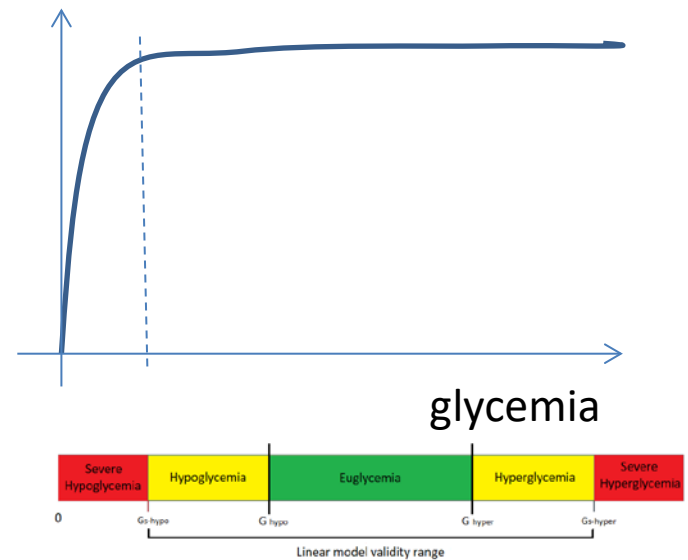
$\theta_2$  : insulin sensitivity factor

$\theta_3$  : sensitivity to digested carbohydrates

$$G \geq 0$$

↓

$$\theta_2 = \theta_2(G)$$



Ref.: Tolic et al.

J. Theor. Biol. (2000) 207, 361-375.

# Mathematical model

$$\dot{G} = \theta_1 - \theta_2 I + \theta_3 D$$

$$I_{basal} = \theta_1 / \theta_2$$

Insulin diffusion : may involve several compartments

Digestion of carbohydrates : may involve several compartments.

Drawback for identification from clinical data: declared meals are questionable

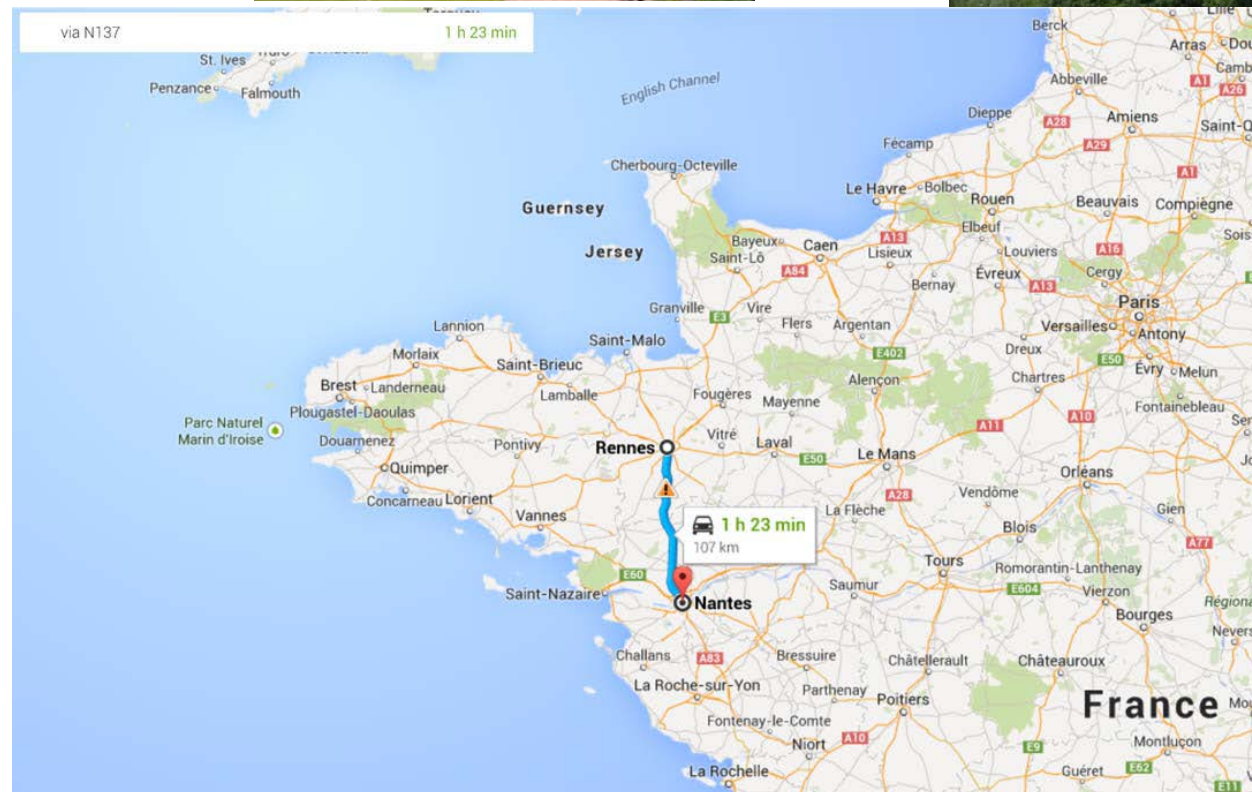
$$\dot{G} = \theta_1 - \theta_2 I + \theta_3 D$$

→ Option 1 :

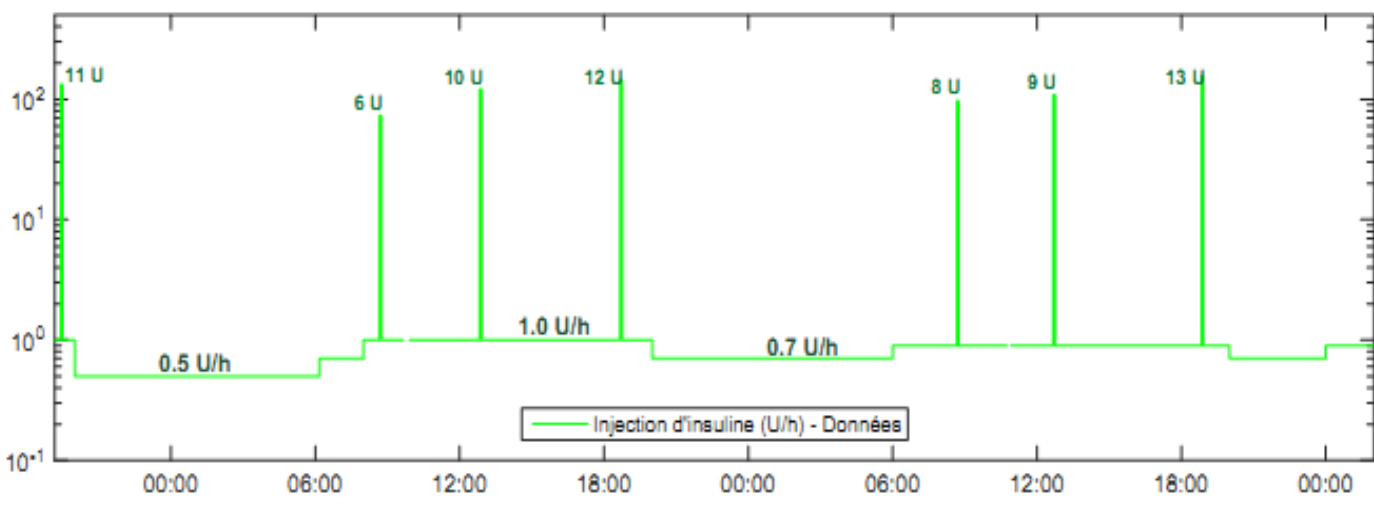
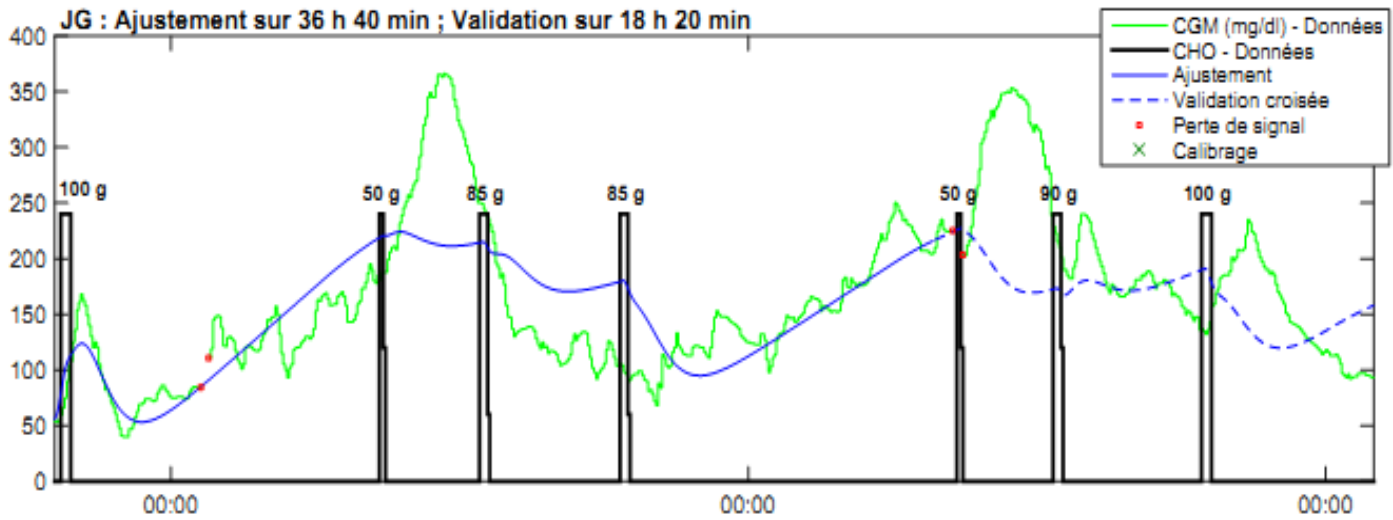
Redefine the time when meals occur, their amplitude...

What is a linear model good for ?

# Clinical data from Nantes hospital and Rennes hospital

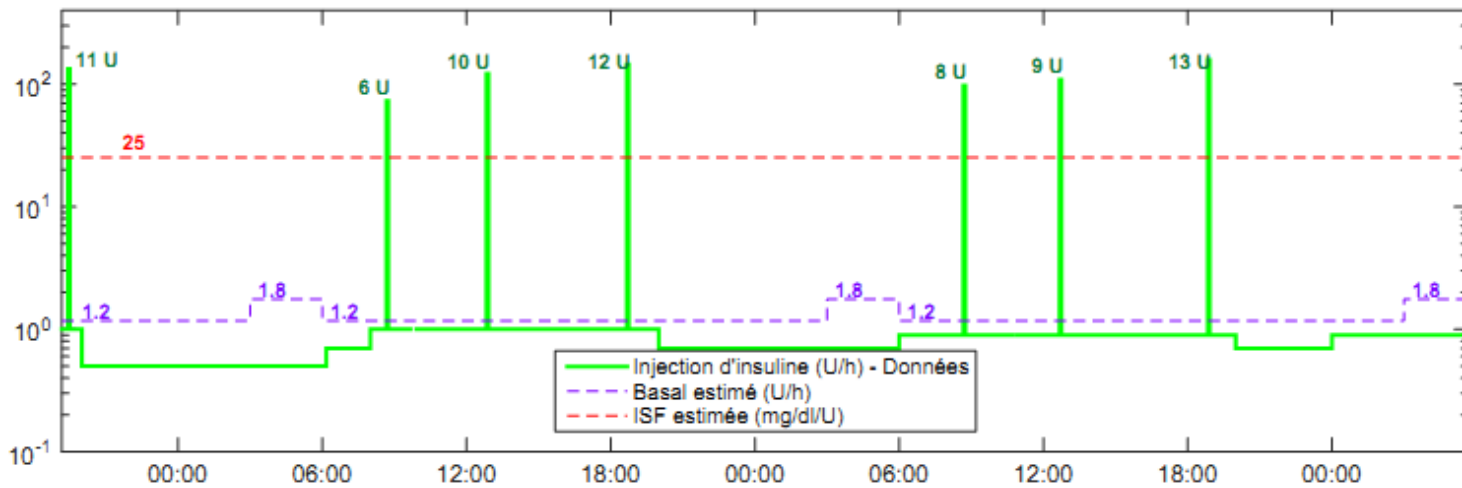
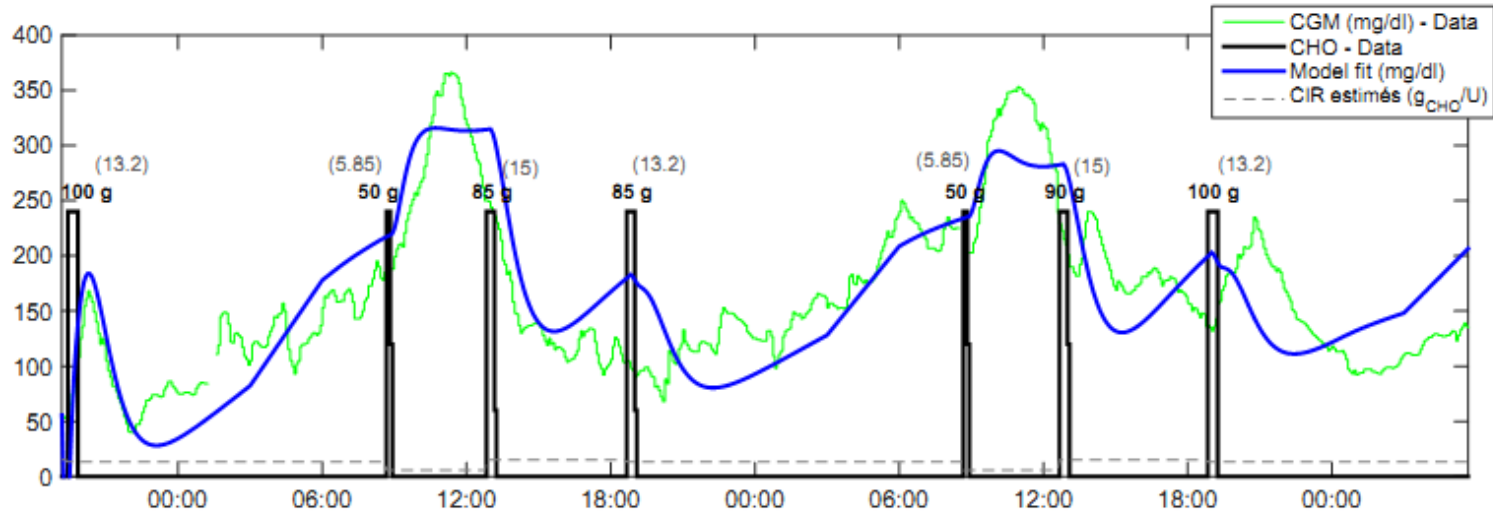


# Identification with constant parameters (and re-positioning of meals)

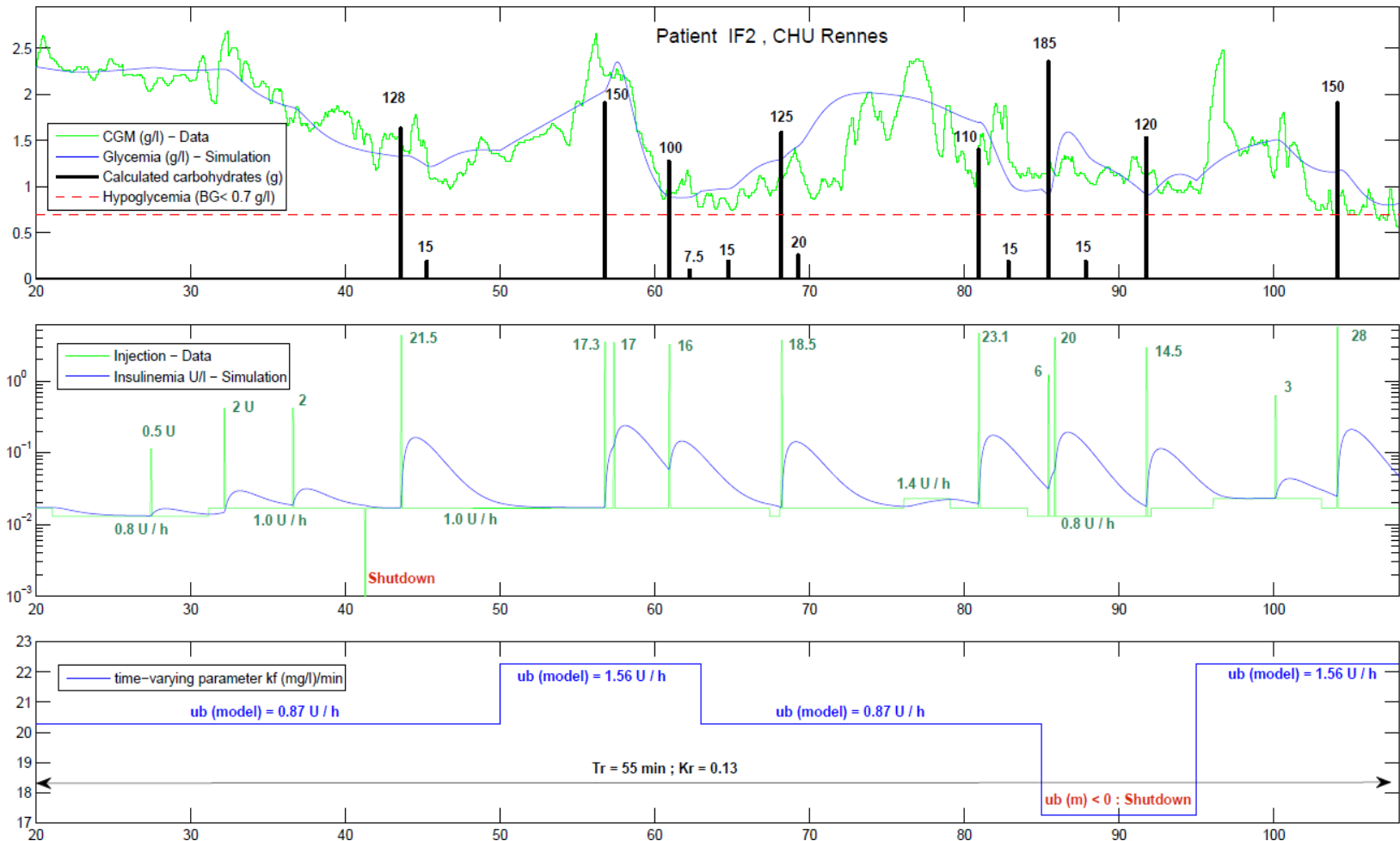




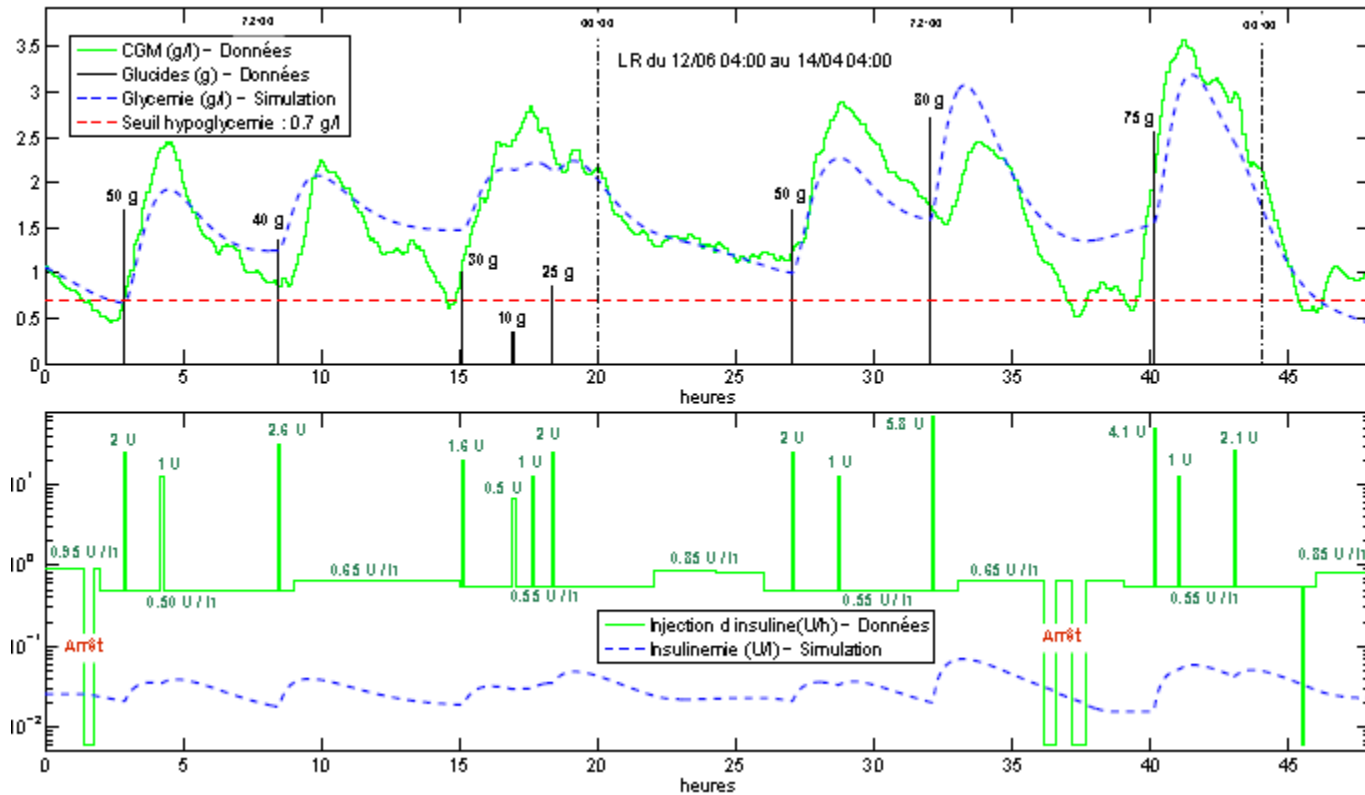
# Identification with varying parameters (and re-positioning of meals)



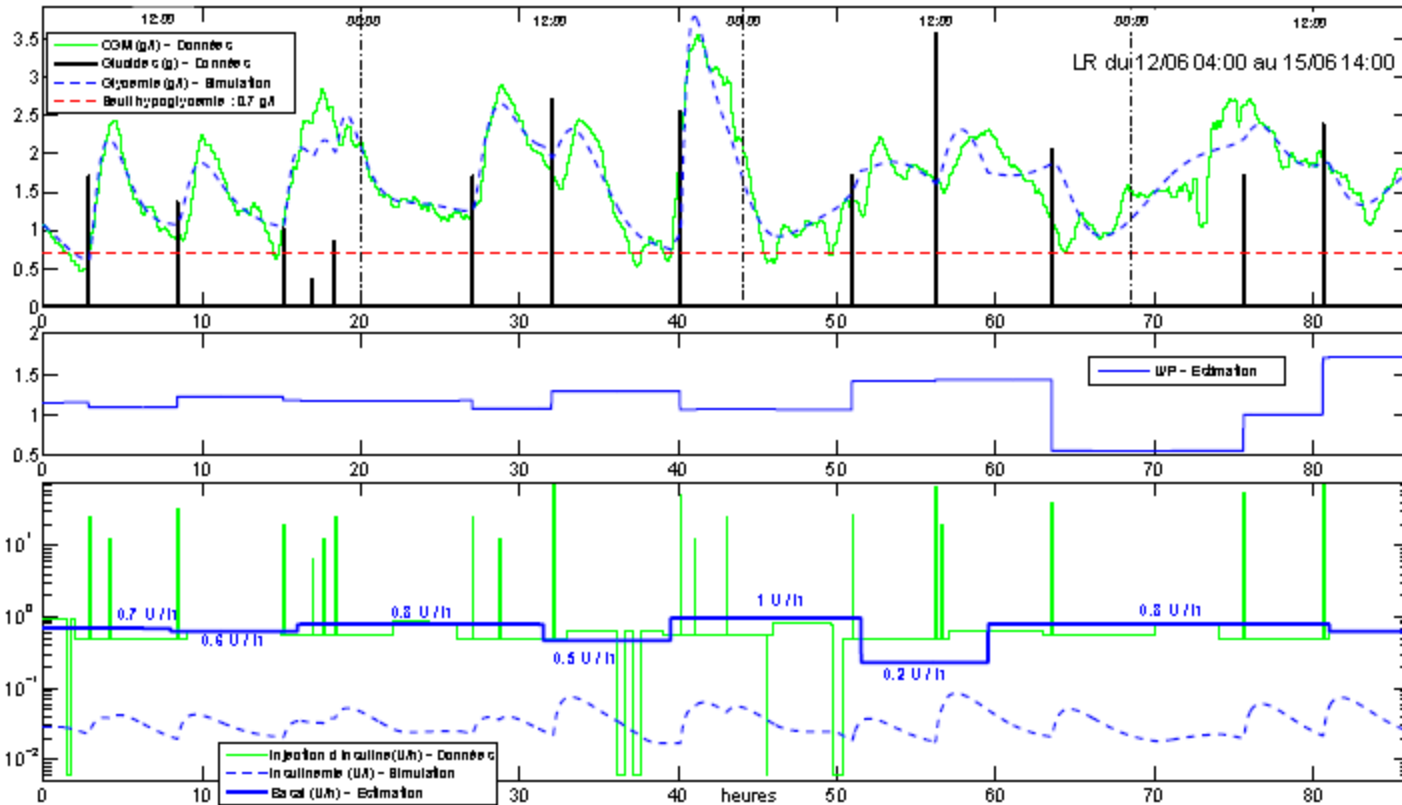
# Patient IF2



# Patient LR



# Patient LR: adaptive estimation



## Criticism:

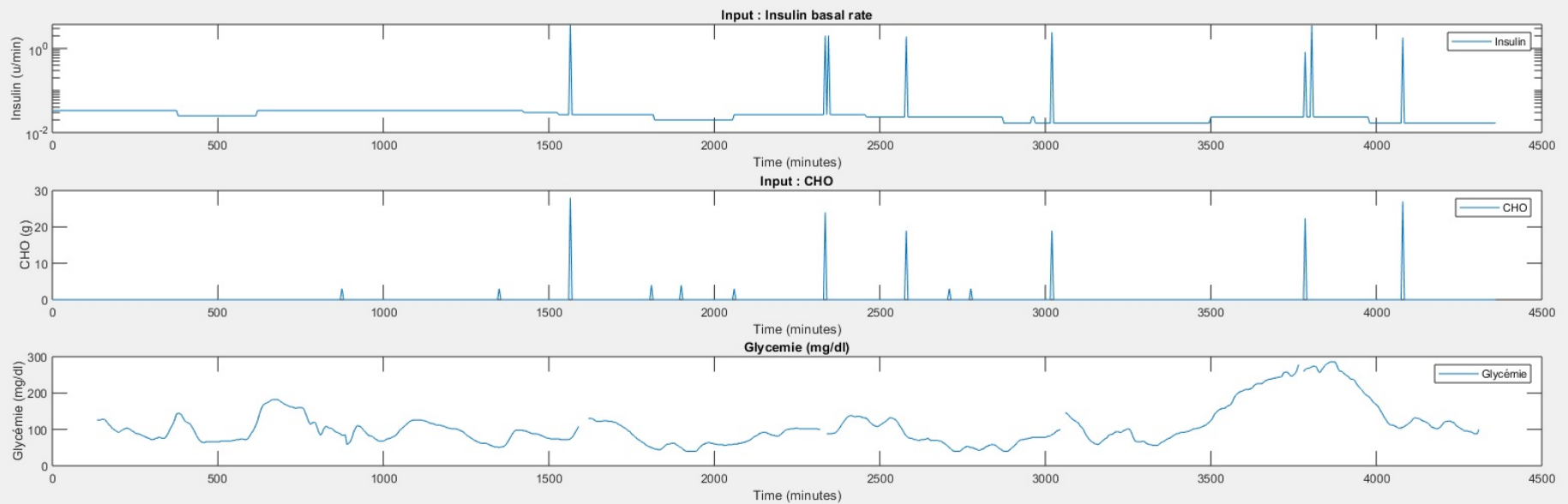
the sequence of meals is used an extra « tuning » for the best fit

Lack of methodology for a suitable  
processing of the meal data 😞

# Towards a methodology for identification

Option 2 :

Select some identifiable events in clinical data as:

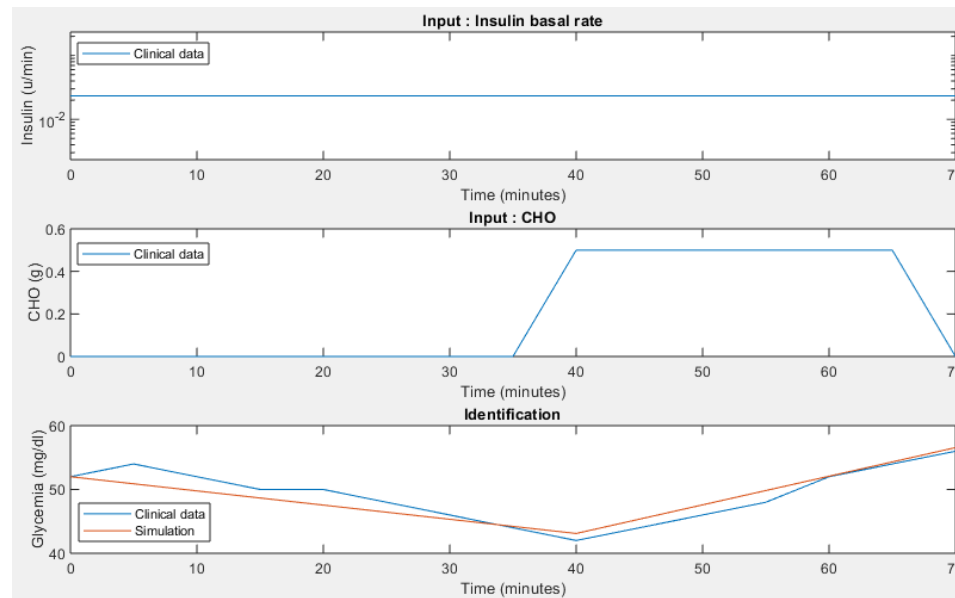


# Towards a methodology for identification

$$\dot{G} = \theta_1 - \theta_2 I + \theta_3 D$$

identification of  $\theta_3$

Special event: when glycemia is too low,  $I = I_{basal} = \theta_1 / \theta_2$   
and  $D \neq 0$



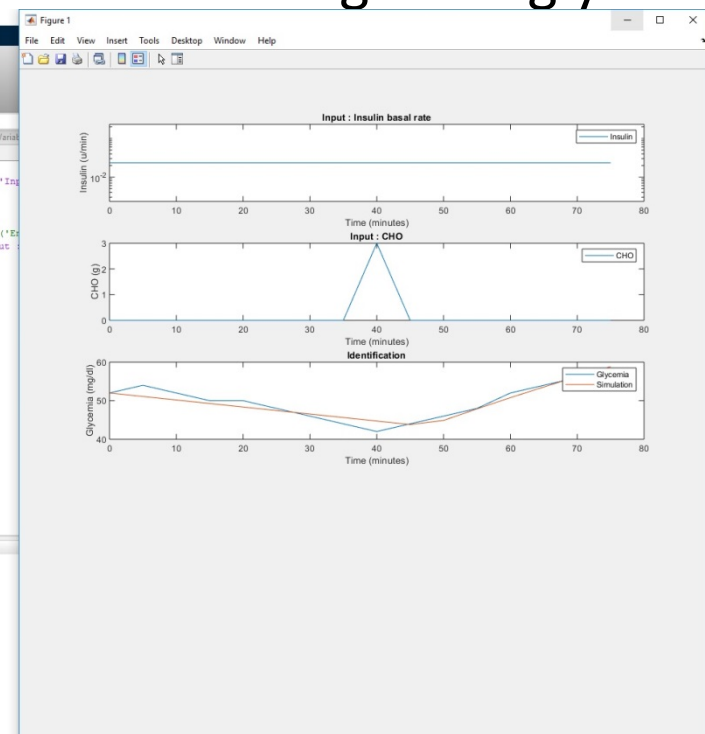
# Towards a methodology for identification

$$\dot{G} = \theta_1 - \theta_2 I + \theta_3 D$$

identification of  $\theta_3$

The inclusion of digestion dynamics  $\dot{D} = -\theta_4 D + \theta_4 M$

allows to identify the « duration » of the effect of the meal  $M$ , according to its glycemic index





# Type of the model

up to some insulin compartments and some digestion compartments:

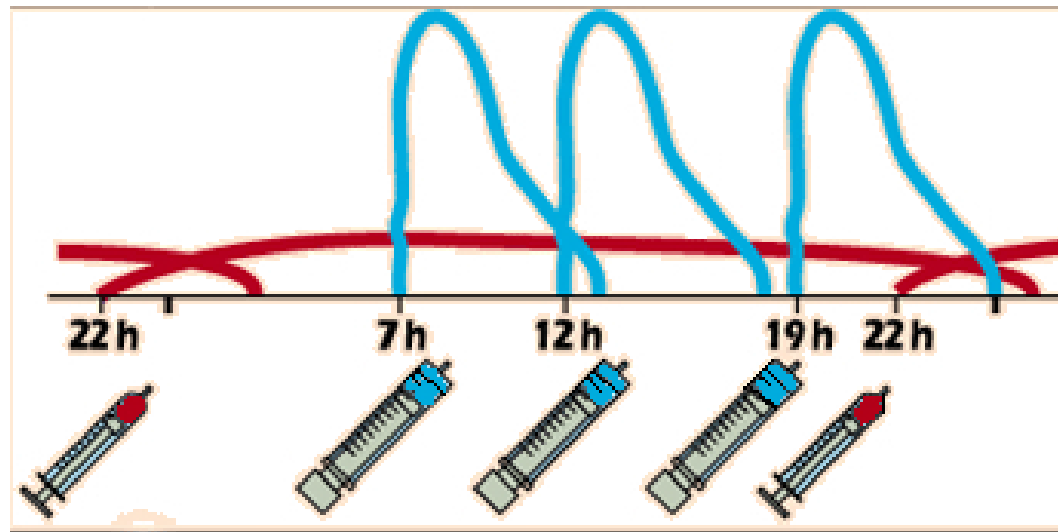
$$\begin{aligned}\dot{G} &= \theta_1 - \theta_2(G).I + \theta_3D \\ \dot{D} &= -\theta_4D + \theta_4M\end{aligned}$$



Depends on the  
glycemic index

# Control

# Real life « manual » control



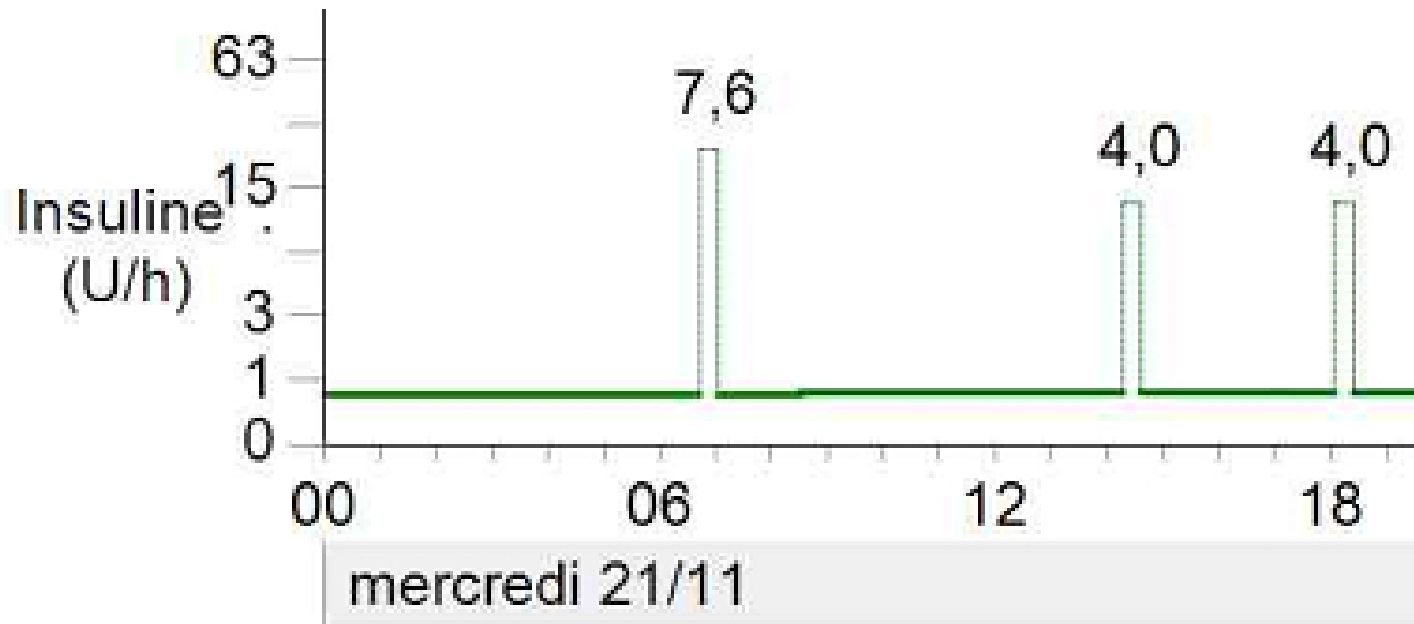
Insulinothérapie  
schéma Basal/Bolus

Slow action insulin

Fast action insulin

# Insulin pump

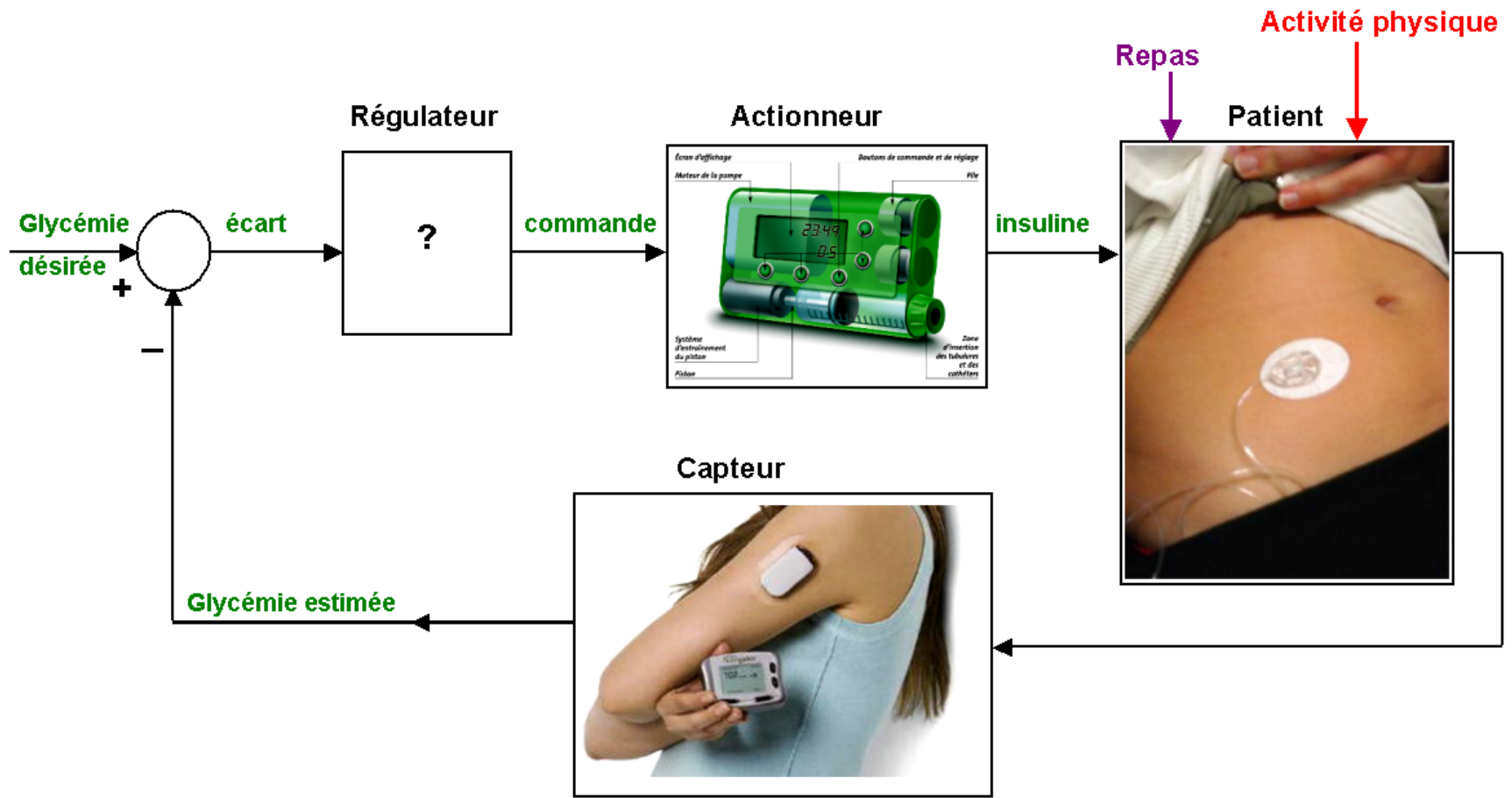
With a single type of insulin



Continuous flow: basal rate

Impulse-like control: bolus

# Closing the loop ?



# Closing the loop ?

- Mainstreams:

Model predictive control (Diabeloop)

PID (Medtronic)

# Control

Dynamic Bolus calculator

derived from the expertise of practitioners

# Bolus calculator

- Derived from real life devices





# Bolus calculator

- Reduces to a state feedback:

Insulin to be injected = insulin required – insulin already injected

$$u = u_{BG} - u_{IoB}$$

$$u = k_1 G - k_2 (I_{SC} + I_P)$$

G = glycemia

I<sub>sc</sub> = sub cutaneous Insulinemia

I<sub>p</sub> = Insulin in plasma

# Bolus calculator properties

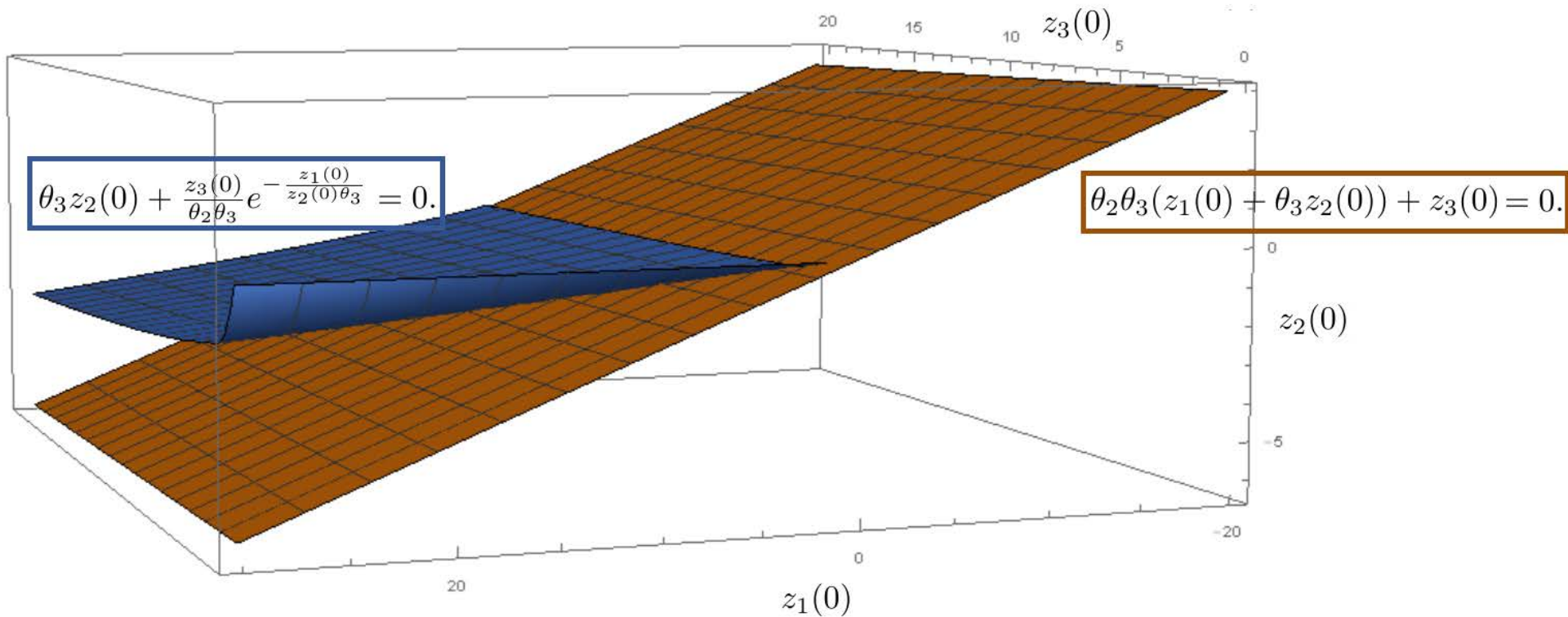
- state feedback: 
$$u = k \left[ \frac{1}{\theta_2} G - \frac{1}{\theta_3} (I_{SC} + I_P) \right]$$
- Defines the largest positively invariant subset !
- Under any other state feedback, the largest PIS shrinks

G = glycemia

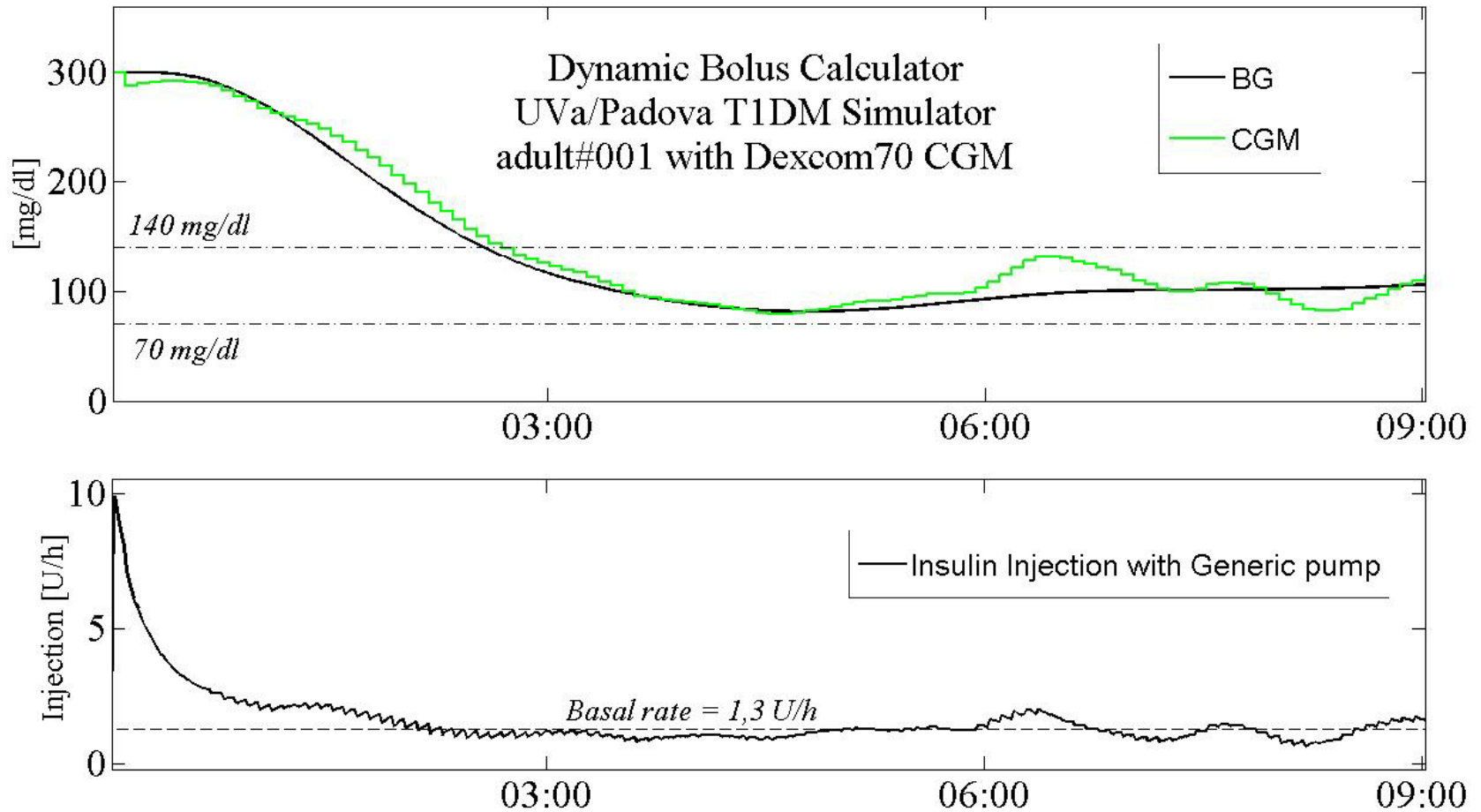
I<sub>sc</sub> = sub cutaneous Insulinemia

I<sub>p</sub> = Insulin in plasma

# Positively Invariant Set



# Dynamic Bolus Calculator



# reference

N. Magdelaine, P.S. Rivadeneira, L. Chaillous, A.L. Fournier-Guilloux, M. Krempf, T. MohammadRidha, M. Aït-Ahmed and C.H. Moog,  
*The Hypoglycaemia-Free Artificial Pancreas Project*,  
IET Systems Biology, 2020, vol. 14, pp. 16-23.

# Conclusions and perspectives

- **What is specific:**
  - Recover the FIT parameters from the model
  - Positive control (hypoglycemia avoidance)
- **Coming next:**
  - Methodology for identification of the basal, CIR,...
  - Clinical trial of identification
  - Prototype

# Conclusions and perspectives

- Main achievement: modelling

N. Magdelaine, L. Chaillous, I. Guilhem, J.Y. Poirier, M. Krempf, C.H. Moog and E. Le Carpentier,

A Long-term Model of the Glucose-Insulin Dynamics of Type I Diabetes,

IEEE Transactions on Biomedical Engineering, (2015).

# Conclusions and perspectives

- Main achievement: modelling
- Implementation of the state feedback (OpenAPS)